The appearance of intracranial hemorrhage at magnetic resonance (MR) imaging depends primarily on the age of the hematoma and the type of MR contrast (ie, T1 or T2 weighted). As a hematoma ages, the hemoglobin passes through several forms (oxyhemoglobin, deoxyhemoglobin, and methemoglobin) prior to red cell lysis and breakdown into ferritin and hemosiderin. Five distinct stages of hemorrhage can be defined: hyperacute (intracellular oxyhemoglobin, long T1 and T2), acute (intracellular deoxyhemoglobin, long T1, short T2), early subacute (intracellular methemoglobin, short T1, short T2), late subacute (extracellular methemoglobin, short T1, long T2), and chronic (ferritin and hemosiderin, short T2). The short T1 of methemoglobin is due to the paramagnetic dipole-dipole interaction. Another paramagnetic property, the magnetic susceptibility effect, is responsible for the short T2 observed when deoxyhemoglobin, methemoglobin, or hemosiderin is intracellular. T2 shortening can also be produced by hemoconcentration and clot retraction. The T2 shortening due to magnetic susceptibility effects is enhanced on higher-field-strength systems and on gradient-echo images and is reduced with "fast spin-echo" MR techniques.

Index terms: Brain, hemorrhage, 10.367 * Brain, MR, 10.1214 * State-of-art reviews

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1 The appearance at magnetic resonance (MR) imaging of most lesions in the brain has a direct correlate in computed tomography (CT). Most lesions, being edematous, appear dark on both unenhanced CT scans and T1-weighted MR images (ie, those acquired with a short repetition time [TR] [approximately 500 msec] and a short echo time [TE] [approximately 20 msec] in which T1 contrast predominates). Such lesions also appear bright on T2-weighted MR images (ie, those acquired with a long TR [approximately 3,000 msec] and a long TE [approximately 80 msec] in which T2 contrast predominates). Hemorrhage, on the other hand, may be bright or dark on T1-or T2-weighted images, depending on the age of the hematoma and the integrity of the red blood cell membrane (1–7). The combination of appearances on T1- and T2-weighted images defines five stages of hemorrhage that can be distinguished with MR imaging (Table).

Much of what has been written on the MR appearance of hemorrhage is contradictory and confusing. Some have suggested that there is no predictable temporal pattern of hemoglobin oxidation (8). Some accept the appearance but have questioned the specific mechanism (9–11). The purpose of this review is to describe the usual pattern of evolving hemorrhage, the proposed mechanisms behind the changes, and the technical factors that affect the MR appearance.

On CT scans, acute intracranial hemorrhage usually becomes hyperattenuating within an hour as the clot retracts. This lasts for several days, and then the hemorrhage fades to become isodense and, eventually, hypodense. On MR images, hemorrhage less than 12 hours old may not be distinguishable from any other edematous mass. Thus, CT should be used to detect hemorrhage in the brain during the first 12 hours after ictus. The subsequent MR appearance of hemorrhage (Table) is an evolving pattern of variable signal intensity that depends on the specific form of hemoglobin present (ie, oxyhemoglobin, deoxyhemoglobin, or methemoglobin) (Fig 1), on whether the red blood cells are intact or lysed, on the operating field strength and the receiver bandwidth, on the type of signal (that is, routine spin echo [SE], fast SE, or gradient echo [GRE]), and on the degree of T1 or T2 weighting (7).

The appearance of hemorrhage depends on the specific intracranial compartment involved: subarachnoid, intraventricular, subdural, epidural, intratumoral, or intraparenchymal. Different zones may also be defined from the inner core to the outer rim of parenchymal hematomas. Because there are unpaired electrons in the heme iron of deoxyhemoglobin and methemoglobin, some basic concepts of paramagnetism must be understood in order to appreciate fully the different T1 and T2 characteristics. Paramagnetic phenomena such as the "electron-proton dipole-dipole interaction" and "magnetic susceptibility effects" both enter into a discussion of the MR appearance of hemorrhage.

PARAMAGNETISM IN HEMORRHAGE

There are two primary mechanisms for T1 and T2 shortening in hemorrhage (Fig 2): "bound-water effects" and "paramagnetic effects" (7,11). Free, "bulk-phase" water (such as cerebrospinal fluid [CSF]) has very high natural motional frequencies (or, alternatively, very short molecular correlation times). Because these natural

Abbreviations: CSF = cerebrospinal fluid, GRE = gradient echo, SE = spin echo, TE = echo time, TR = repetition time.
motional frequencies are much higher than the Larmor frequencies used in MR imaging. T1 relaxation is inefficient and the T1 relaxation time of CSF is longer than that of any other substance in the body (approximately 2,700 msec) (11).

When protein is added to pure water, the polar water molecules are attracted or "bound" to the charged side groups of the protein, forming a hydration layer. Water in this hydration layer environment has longer molecular correlation times and shorter T1 relaxation times than pure CSF (ie, approximately 400–1,000 msec, depending on protein concentration). Thus the T1 of nonparamagnetic, proteinaceous oxyhemoglobin is much less than that of CSF and approaches that of brain parenchyma (11).

Considerably greater T1 shortening is possible due to the dipole–dipole interaction resulting from paramagnetic substances such as gadolinium or methemoglobin in aqueous solution. Such paramagnetic substances (13) (defined by the presence of unpaired electrons) may shorten the T1 of aqueous solutions into the several hundred millisecond range, which is considerably shorter than that possible with diamagnetic species (ie, those not having unpaired electrons).

A similar statement can be made for T2 shortening. Proteinaceous solutions of sufficient concentration can bind sufficient water to cause observable T2 shortening compared with that of brain. Such "solutions" are really more like mucinous gels (11) and contribute to the T2 shortening observed at high hematocrit as water is resorbed from a hematoma (7). Substantially greater T2 shortening is observed from the magnetic susceptibility effects resulting from compartmentalization of paramagnetic deoxy- or methemoglobin inside intact red blood cells (7). In general, the greater the number of unpaired electrons, the greater the paramagnetic effect (14).

Because the interaction between the dipole of the unpaired electrons and that of a hydrogen nucleus falls off as the sixth power of the distance between them, hydrogen nuclei must be able to approach the paramagnetic center within a distance of 3 Å (13), or there will be negligible T1 shortening. In methemoglobin the water molecules can closely approach the heme iron, but in deoxyhemoglobin they cannot because of the configuration of the protein. Therefore, methemoglobin demonstrates paramagnetic T1 shortening but deoxyhemoglobin does not.

Paramagnetic substances also become more strongly magnetized than diamagnetic substances when placed in a magnetic field. Exactly how magnetized a substance becomes is quantified by the magnetic susceptibility coefficient, which is the ratio of the induced to the applied magnetic field. Paramagnetic substances such as hemosiderin have high magnetic susceptibilities and become more magnetized than diamagnetic substances when placed in an external magnetic field. This leads to focal "hot spots," which create local regions of magnetic nonuniformity. These in turn lead to rapid dephasing of spins and signal loss on T2*-weighted GRE images (14–18). As water protons diffuse through these magnetically nonuniform regions, they lose phase coherence in proportion to the interecho time, which also decreases the signal intensity on T2-weighted SE images (1,17,19). Because the induced field (and thus the induced nonuniformity) is proportional to the strength of the applied magnetic field (through the magnetic susceptibility coefficient), both T2* and T2 shortening are greater at higher field strengths (1,5,15). To the extent that dephasing results from diffusion through the field gradients (20) resulting from these nonuniformities, T2 decreases as the square of the field strength (1) at constant bandwidth. As the receiver bandwidth is decreased on systems of low and middle field strength, however, the sensitivity to susceptibility effects is increased somewhat, partially reflecting the longer TEs required to accommodate the longer echo sampling times. As the time available for diffusion decreases—for example, with the short echo spacing of "fast SE"—the sensitivity to this magnetic susceptibility decreases (21,22), although some workers main-
TEMPORAL PHASE | BULK MAGNETIZATION | T2 RELAXATION
--- | --- | ---
Hyperacute | $H_2O$ oxy | TE
Acute | $H_2O$ deoxy | TE
Subacute | $H_2O$ met | TE

**Figure 2.** Mechanisms of T1 and T2 shortening in hemorrhage.

**Figure 3.** T2 shortening in fresh hematomas. T2 relaxation time of a hematoma depends on its temporal phase (hyperacute: first few hours; acute: 1–3 days; subacute: >3 days). In all phases, bulk magnetization of the extracellular space is the same (arrow of constant size). Bulk magnetization of the intracellular compartment (within intact red blood cells) changes during the evolution of the hematoma. Oxyhemoglobin (during the hyperacute phase) has low induced magnetization because of its low magnetic susceptibility. This results in similar induced magnetization in the intracellular and extracellular environments such that water diffusing across the red blood cell membrane experiences a constant field. For this reason, there is no dephasing due to diffusion and therefore little T2 relaxation. During the acute phase, magnetically susceptible deoxyhemoglobin is formed, resulting in a higher magnetization within the red blood cell than in the surrounding extracellular space. The magnetic field gradient experienced by water molecules diffusing across the red blood cell membrane results in additional dephasing and T2 shortening. Since the red cells are still intact during the early subacute phase when methemoglobin is formed, even greater dephasing will occur due to the somewhat higher magnetization induced in methemoglobin with five unpaired electrons compared to deoxyhemoglobin, which has four.

**OXIDATION OF HEMOGLOBIN**

The variable MR appearance of hemorrhage (Fig 4) depends on the structure of hemoglobin and its various oxidation products (28). In the circulation, hemoglobin alternates between the oxy and deoxy forms. As the blood passes through the high oxygen environment of the lungs, molecular oxygen ($O_2$) is bound, forming oxyhemoglobin. When the blood then passes through the lower oxygen environment of the capillaries, the $O_2$ is given off, forming deoxyhemoglobin. To bind oxygen reversibly, the iron in the hemoglobin (the "heme iron") must be maintained in the reduced, ferrous (Fe²⁺) state. When the red blood cell is removed from the high oxygen environment of the circulation, deoxyhemoglobin undergoes denaturation to methemoglobin, and the heme iron becomes oxidized to the ferric (Fe³⁺) form.

Changes in the conformation of the hemoglobin molecule result from changes in the oxidation state of the heme iron. The heme iron is normally held in a nonpolar crevice in the hemoglobin molecule. It is held by a covalent bond to a histidine attached at the F8 position of the globin chain and by four hydrophobic van der Waals forces to nonpolar groups on the globin molecule. The sixth coordination site of the heme iron is occupied by molecular oxygen in oxyhemoglobin and is vacant in deoxyhemoglobin (Fig 1). In methemoglobin, the sixth coordination site is occupied by either a water molecule or a hydroxyl ion, depending on whether the methemoglobin is in the acid or base form, respectively (6). At physiologic pH, the acid form predominates. With continued oxidative denaturation, methemoglobin is converted to derivatives known as hemichromes (28). The iron in these compounds remains in the ferric state. An alteration of the tertiary structure of the globin molecule causes that the sixth coordination site of the heme iron becomes occupied by a ligand.
from within the globin molecule (the distal histidine at E7).

After red blood cell lysis, the hemo-
globin is broken down into the heme
iron and the globin molecule. The
iron is initially stored as ferritin, which
is water-soluble ferric hydrox-
ide-phosphate micelles attached to
the iron storage protein, apoferitin
(29,30). With localized iron overload
(13) and depletion of apoferitin, he-
mosiderin is formed, which repre-
sents water-insoluble clumps of ferri-
tin particles (29).

While the oxidation state of the
heme iron has everything to do with
its function, it has nothing at all to do
with the appearance of blood on MR
images. The MR appearance depends
on whether there are unpaired elec-
trons, that is, on whether the species
is paramagnetic. The magnetic prop-
erties of hemoglobin were initially
described almost 150 years ago by Far-
aday (31) and subsequently by Paul-
ing and Coryell (32). Basically, oxyhe-
moglobin and the hemichromes are
diamagnetic—that is, they have no
unpaired electrons—and deoxy- and
methemoglobin are paramagnetic.
Deoxyhemoglobin has four unpaired
electrons and methemoglobin has
five. Since seven unpaired electrons
is the maximum possible (eg, gadolin-
ium), deoxy- and methemoglobin are,
indeed, quite paramagnetic.

Paramagnetism per se does not en-
sure T1 shortening in aqueous solu-
tion; the paramagnetic centers must
also be accessible to surrounding wa-
ter protons. Quantitation of T1 shorten-
ing requires consideration of the
magnitude of the magnetic moment
of the paramagnetic dipole (that is,
the number of unpaired electrons),
the electron spin relaxation time, the
concentration of paramagnetic di-
poles, the average distance from sur-
rrounding water protons, and the rela-
tive motions of the protons and the
paramagnetic centers (6,13). Theories
of proton relaxation by paramagnetic
solute agents are based on transla-
tional diffusion and the distance of closest ap-
proach of the proton and paramag-
netic ions, which determines an
"outer sphere" of influence (33). It
has also been shown that there can be
a contribution to the relaxation from
exchange between the solvent and
water ligands in the first coordination
sphere of the paramagnetic ion, that
is, "inner-sphere effects" (33).

Although deoxyhemoglobin is
paramagnetic, it does not cause T1
shortening. Because the electron spin
relaxation time of deoxyhemoglobin
is very short and because water mole-
cules are unable to approach the heme
iron within a distance of 3 Å, the T1 of
an aqueous solution of deoxyhem-
globin is not short (34). In fact, the T1
of an acute hematoma is prolonged
(compared to brain) due to the higher
water content (35). The frequencies
corresponding to the electron spin re-
relaxation time of methemoglobin, on
the other hand, are much closer to the
Larmor frequencies used in MR imag-
ing (32). Also water molecules are bet-
ter able to approach the paramagnetic
center in methemoglobin than in de-
oxyhemoglobin (33). Thus, methemo-
globin causes significant T1 shorten-
ing in aqueous solutions, while deoxy-
hemoglobin does not.

**EVOLVING PARENCHYMAL
HEMATOMA**

For hemorrhage to be staged prop-
erly with MR imaging, both T1- and
T2-weighted images must be ac-
quired. Five stages of an evolving he-
matoma can be described (7): hyper-
acute (intracellular oxyhemoglobin,
first few hours), acute (intracellular
dehemoglobin, 1–3 days), early
subacute (intracellular methemoglobin,
about 3–7 days), late subacute
(extracellular methemoglobin, more
than 7 days), and chronic (older than
2 weeks) (Table).

During the first few hours (hyper-
acute phase), the hematoma consists
of a mixture of oxy- and deoxyhemo-
globin (Fig 5), initially as a liquid sus-
pension of intact red blood cells and,
as thrombosis progresses and plasma
is resorbed, an increasingly solid con-
glomerate of intact red blood cells
(1,25–27). Over the next few days
(acute phase), the hematoma consists
primarily of deoxyhemoglobin within
intact red blood cells (1) (Fig 6). The
term "hyperacute" was first adopted

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**Figure 4.** Factors affecting the MR appearance of hemorrhage.

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**Figure 5.** Hyperacute hemorrhage (stagnant oxyhemoglobin) in a 35-year-old heroin addict who had experienced cardiopulmonary arrest immediately prior to the acquisition of these images. (a) Proton-density-weighted MR image (SE 3,000/25 [TR msec/TE msec]) demonstrates high intravascular signal intensity due to complete absence of motion in the jugular veins (large arrows) and carotid arteries (small arrows). (b) T2-weighted (SE 3,000/80) axial MR sec-
tion through the same level as a demonstrates intravascular hyperintensity (arrows) due to
long T2 of unclotted intracellular oxyhemoglobin. (The patient was subsequently resuscitated.)
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begins in presence "acute." Seen as deoxyhemoglobin, (36)

Figure 6. Acute hematoma in an 80-year-old man with a 3-day history of "memory loss." (a) T1-weighted (SE 500/20) axial MR section demonstrates central area isointense to brain (large arrow) with peripheral rim of hyperintensity (small arrow). (b) T2-weighted (SE 3,000/80) axial MR image through the same level as (a) demonstrates marked hypointensity (arrow) on this 1.5-T image. The combination of findings indicates that the hematoma has a markedly shortened T2 with a small peripheral component of shortened T1. The 3-day history and the presence of persistent mass effect and edema indicate that the majority of this hemorrhage is in the intracellular deoxyhemoglobin form with early oxidation to methemoglobin at the periphery.

Figure 7. Hemorrhagic metastases on high-field-strength, GRE images. This 55-year-old woman presented with headaches without focal neurologic findings. Subsequent work-up revealed hemorrhagic metastases to the brain from small cell carcinoma of the lung. (a) Mildly T2-weighted (SE 2,500/30) axial MR section demonstrates a few scattered abnormalities. (b) MR image obtained with gradient-recalled acquisition in the steady state (GRE 200/80, 10° flip angle) demonstrates multiple additional foci of low intensity due to additional sensitivity to magnetic susceptibility effects.

(36) to describe the stage preceding deoxyhemoglobin, which was defined as "acute" by Gomori et al (1). Both hyperacute and acute hematomas seen on MR images appear hyperattenuating on CT scans and are labeled "acute."

During the subacute period, which begins after several days, deoxyhemoglobin undergoes oxidative denaturation, forming methemoglobin (6). Early in this phase (Figs 7, 8), the red blood cells are intact. Later in this phase (after approximately 1 week), red cell lysis occurs (Fig 9).

In parenchymal hematomas, modified macrophages (microglia or gitter cells) move in from the periphery by the end of the 2nd week and remove the iron from the extracellular methemoglobin (7). This marks the beginning of the chronic phase when the heme iron is deposited at the periphery as a rim of hemosiderin and ferritin (27) within macrophages (Fig 9) (1). The center of the hematoma is eventually left with non-iron-containing, nonparamagnetic heme pigments, such as hematoxident (37).

A note of caution: Although it is useful to describe the evolution of a hematoma in these well-defined stages, in fact the stages may coexist (8). For example, at the time hemosiderin and ferritin are first deposited at the periphery of a hematoma (indicating the beginning of the chronic stage), free methemoglobin is present in the outer core (late subacute stage) (Fig 9) and intracellular deoxyhemoglobin or even oxyhemoglobin may still be found in the inner core from the acute and hyperacute stages, respectively. By convention, the hematoma is described in terms of the most mature form of hemoglobin that is present (7).

Hyperacute Phase

On short TR/TE, T1-weighted images, hyperacute hematomas (a few hours old) are predominantly oxyhemoglobin and are iso- to hypointense compared with brain due to their longer T1 times, reflecting their higher water content (25–27). The T2 relaxation time reflects both the fluidsolid character of the fresh hematoma (Fig 5) (24–27) and the relative amounts of oxyhemoglobin and deoxyhemoglobin. Ninety-five percent of arterial blood is oxyhemoglobin (29), which is diamagnetic and does not cause T2 shortening. Because most nontraumatic hemorrhages are arterial (such as that from aneurysms, and/or microaneurysms in hypertension), there may be no significant T2 shortening initially (Fig 5). The minimum concentration of deoxyhemoglobin that produces visible T2 shortening depends on the field strength (1), the bandwidth, and the imaging technique, with GRE studies being more sensitive than SE studies (14–18). It should be stressed, however, that during the first few hours after a hemorrhage, MR is less sensitive than CT.

Acute Phase

After the initial 24 hours, deoxyhemoglobin is normally found within clotted, intact red blood cells (1,18). As noted earlier, although deoxyhemoglobin is magnetically susceptible, it
does not cause T1 shortening. T2 shortening results from the dephasing due to diffusion of water molecules in and out of the red blood cell (Fig 6). Since the magnetic susceptibility effects increase with field strength, the low-intensity appearance of an acute hematoma on T2-weighted images may be more obvious at higher field strengths (1). Low flip angle, T2*-weighted, GRE images are also more sensitive to susceptibility effects than T2-weighted SE images (14–18) (Fig 7). Since high field strength and GRE techniques increase the sensitivity to magnetic susceptibility effects through different mechanisms, they are additive (14) and produce marked signal loss when applied together.

During both the hyperacute and acute phases, progressive concentration of red blood cells by thrombosis also causes T2 shortening (Fig 2) (24,26,38,39). This reflects both clot retraction and increasing hematocrit (24,26,27). Formation of the fibrin clot (from polymerization of fibrinogen) and clot retraction (by platelets) both shorten T2 (24). Such effects can be seen in plasma clots alone without any magnetically susceptible species (24). Prior to clot retraction, therefore, T2 shortening may be minimal (25,26).

The T2 shortening that results from increasing hematocrit increases with field strength, like the magnetic susceptibility effects. The mechanism reflects increasing protein concentration and binding of water protons (11,40,41). T2 shortens progressively as the hematocrit approaches 100% (24). Dehydration of red blood cells is also known to occur during the acute phase and can cause a selective decrease in T2 (42–46).

It should be stressed that it may not be possible to distinguish among the various mechanisms that lead to T2 shortening in acute hemorrhage. Specifically, the signal intensity loss noted in about 24 hours on long TR/TE T2-weighted images may be

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**Figure 8.** Early subacute hematoma in a 30-year-old man with known arteriovenous malformation and 4-day history of obtundation. (a) T1-weighted (SE 500/20) axial MR image demonstrates hyperintensity in hematoma within right parietal lobe (large arrow) and right lateral ventricle (small arrow). Note also flow voids of dilated arterial feeders of the arteriovenous malformation (arrowheads). (b) T2-weighted (SE 3,000/80) axial MR image demonstrates central hypointensity within both right parietal and right lateral ventricular hematomas. The combination of high signal intensity on the T1-weighted image and low signal intensity on the T2-weighted image is indicative of intracellular methemoglobin.

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**Figure 9.** Late subacute hemorrhage 3 weeks following head trauma to a 64-year-old man. (a) T1-weighted (SE 500/20) axial MR image demonstrates high-intensity right convexity subdural hematomas (small arrows), as well as right subfrontal parenchymal hematoma (large arrow). The ventricles are dilated due to associated communicating hydrocephalus from subarachnoid hemorrhage. (b) Proton-density–weighted (SE 3,000/20) axial MR image demonstrates persistent hyperintensity of the subdural and parenchymal hematomas relative to lower intensity CSF. A hemosiderin rim (arrowheads) is now becoming visible around the parenchymal hematoma. (c) T2-weighted (SE 3,000/80) axial MR image demonstrates persistent hyperintensity of the subdural and parenchymal hematomas, which are now isointense with hyperintense CSF. The combination of high signal intensity on the T1-weighted image with persistent high signal intensity on the T2-weighted image is indicative of extracellular methemoglobin. The hemosiderin rim surrounding the parenchymal hematoma is more apparent with additional T2 weighting, indicating the beginning of the chronic stage.
due to deoxygenation, hemoconcentration, red blood cell dehydration, and/or clot retraction. Further, the relative influence of these factors on T2 shortening depends on the operating field strength (Fig 2) (24).

Early Subacute Phase

The subacute phase is defined by the oxidation of deoxyhemoglobin to methemoglobin (6). In the early subacute phase, the red blood cells are still intact (47). With the formation of methemoglobin, T1 is markedly shortened due to a dipole-dipole interaction, resulting in increased intensity on T1-weighted images (6,47) (Fig 8). For parenchymal hematomas, the formation of methemoglobin begins peripherally (Fig 6) due to "intrinsic tissue factors" (48). In addition, oxygen is needed for the oxidation of the heme iron, and the oxygen level is higher in the normal surrounding brain than in the center of the hematoma. Later, the center becomes oxidized to methemoglobin as well. Interestingly, the pattern of methemoglobin formation is exactly the opposite for partially thrombosed intracranial aneurysms, as the oxygen tension is higher in the central lumen than at the periphery (47).

In the early subacute phase, the red blood cells are still intact. Since methemoglobin is magnetically susceptible, the middle of the red cell becomes more magnetized than the plasma on the outside. Thus, the magnetic nonuniformity that causes T2 shortening with intracellular deoxyhemoglobin persists with intracellular methemoglobin.

T1-weighted imaging is better suited to distinguish acute hemorrhage (long T1) from subacute hemorrhage (short T1). Since methemoglobin has five unpaired electrons (compared to four for deoxyhemoglobin), the T2 of the hematoma should be additionally shortened in the transition from the acute to early subacute phase, although this may be difficult to document.

Late Subacute Phase

Late subacute hemorrhage is bright on both T1- and T2-weighted images. By the late subacute phase, red cell lysis has occurred. On T1-weighted images, both early and late subacute hemorrhage appears bright, since water molecules can pass freely across the red blood cell membrane. As lysis occurs, the T2 shortening that had resulted from compartmentalization of methemoglobin is lost (Fig 9). In addition, the high water content of the lysed red cells leads to increase in both T2 and proton density (compared to brain) (49). Obviously, T2-weighted images are necessary for accurate distinction between early (short T2) and late (long T2) subacute hemorrhage (7).

Chronic Phase

In the chronic phase, paramagnetic hemosiderin and ferritin (which have high magnetic susceptibilities) are found within macrophages in a dark ring surrounding the hematoma on T2-weighted images (Fig 9) (30). For ferritin and hemosiderin to be formed, red blood cells containing methemoglobin must first lyse (30). Thus, initially there is always a bright
ring of free methemoglobin just inside the darker hemosiderin ring on T2-weighted images. Eventually the hematoma is reduced to a hemosiderin-lined slit (Fig 10). Like deoxyhemoglobin, intracellular, paramagnetic hemosiderin causes preferential T2 shortening (1).

SUBDURAL AND EPIDURAL HEMATOMAS

Like parenchymal hemorrhage, subdural hematomas have five stages of evolution and thus five different appearances on MR images (7,50,51). Since the dura is so well vascularized, however, the oxygen tension remains high, and the temporal progression from one stage to the next is slower in the extraxial compartment than in the brain itself (50). The first four stages are the same as for a parenchymal hematoma with the same T1 and T2 characteristics. The chronic stage is characterized by continued oxidative denaturation of methemoglobin, forming nonparamagnetic hemichromes (28). The T1 of such compounds is greater than that of paramagnetic methemoglobin; thus the intensity of chronic subdural hematomas is less than that of subacute subdural hematomas, particularly on T1-weighted images. Chronic subdural hematomas (Fig 11) are less intense than subacute subdural hematomas (Fig 9) but more intense than CSF due to their higher protein content (40,50,51). In the extraxial compartments during the chronic phase, there is no hemosiderin rim per se because there are no tissue macrophages to surround the hematoma. In the case of recurrent bleeding into a subdural hematoma, however, there may be hemosiderin staining of the membrane, which forms along the inner border of the subdural collection. Like the hemosiderin surrounding a parenchymal hematoma, this will also turn dark on T2-weighted images.

Figure 12. Early subacute subarachnoid hemorrhage in a 32-year-old woman with bleeding from ruptured posterior inferior cerebellar artery aneurysm 2 weeks earlier. (a) T1-weighted (SE 450/22) sagittal MR image demonstrates abnormal high signal intensity in the pontine and medullary cisterns (arrow). (b) T1-weighted (SE 450/22) axial MR image through the caudal medulla demonstrates abnormal hyperintensity anterior to the brain stem (arrow). (c) Proton-density–weighted (SE 3,000/22) axial MR image shows no significant abnormality as the subarachnoid thrombus has become isointense with CSF. (d) T2-weighted (SE 3,000/90) axial MR image demonstrates marked hypointensity (arrow) in the subarachnoid thrombus compared to the hyperintense CSF around it. The combination of high signal intensity on the T1-weighted image and low signal intensity on the T2-weighted image is indicative of early subacute hemorrhage.

Figure 13. Superficial siderosis in a 65-year-old man following subarachnoid hemorrhage. (a) T2-weighted (SE 3,000/80) axial MR image demonstrates linear hypointensity (arrows) involving posterior left frontal gyrus due to superficial siderosis from previous subarachnoid hemorrhage. (b) T1-weighted (SE 500/20) axial MR image demonstrates methemoglobin within subacute subarachnoid thrombus in central sulcus (arrow). (c) T1-weighted (SE 500/20) left parasagittal MR image demonstrates methemoglobin extending into sulcus (arrow), confirming subarachnoid (vs subdural) location.
of a subdural hematoma with recurrent bleeding, the hemosiderin-stained membrane can simulate the dura, potentially leading to the mistaken diagnosis of epidural hematoma in morphologically atypical cases.

SUBARACHNOID AND INTRAVENTRICULAR HEMORRHAGE

Subarachnoid and intraventricular hemorrhage differs from intraparenchymal, subdural, or epidural hemorrhage in that it is mixed with CSF. Like the extraaxial hematomas, however, subarachnoid and intraventricular hemorrhage have high ambient oxygen levels and thus "age" more slowly than parenchymal hematomas (Fig 12).

Immediately after subarachnoid hemorrhage, there is a small decrease in T1 (6,52-54), reflecting the increase in hydration-layer water (45) due to the higher protein content of the bloody CSF. This leads to subtle increase in signal intensity in the CSF on T1- and proton-density-weighted images ("dirty CSF") (52-54). As has been shown in vitro (6), significant quantities of methemoglobin are not formed until several days after the hemorrhage. Several days to a week after the ictus, signal intensity increases in the subarachnoid space due to methemoglobin formation (Fig 12).

In cases of milder subarachnoid hemorrhage, the red blood cells may be resorbed by the time significant methemoglobin formation would have occurred, and, therefore, the anticipated short T1 appearance will not be seen. For these reasons, CT is advocated for the early diagnosis of subarachnoid hemorrhage (6,7). A short T2 appearance is observed in subarachnoid or intraventricular hemorrhage when massive bleeding has occurred, in which case a fluid-fluid level or a subarachnoid or intraventricular thrombus may be present (Figs 8, 12) (6,53). In chronic, repeated subarachnoid hemorrhage, hemosiderin may be seen staining the leptomeninges, leading to a short T2 appearance known as "superficial siderosis" (55) (Figs 13, 14).

INTRATUMORAL HEMORRHAGE

Hemorrhage is common in the higher grade gliomas and certain highly vascular metastases, for example, melanoma (Fig 15), choriocarci-
The diagnosis of a neoplastic source of hemorrhage may be difficult to make in the subacute setting. Since methemoglobin is already hyperintense, it may be difficult to appreciate marginal gadolinium enhancement against an already intense background. In such cases, CT with and without contrast material may be useful, as the subacute hemorrhage is usually hypointensifying at CT. Similarly, during the acute phase of neoplastic hemorrhage, the hyperintensity at CT may make marginal enhancement difficult to appreciate; simultaneously, the background deoxyhemoglobin on a T1-weighted MR image is hypointense, facilitating the detection of marginal enhancement with gadolinium.

Early pial metastases are notoriously difficult to detect without gadolinium, due to the lack of associated vasogenic edema and T2 prolongation (56). Should these metastases be hemorrhagic (Fig 15), they may actually be hypointense on T2-weighted images due to intracellular deoxyhemoglobin and methemoglobin.

Whether a hematoma results from a tumor or other source, fluid-fluid levels may be seen. The dependent portion is often hypointense on T2-weighted images due to the presence of intact red blood cells containing deoxyhemoglobin or methemoglobin. The nondependent fluid is more intense than CSF on proton-density- and T2-weighted images but not as intense as methemoglobin on T1-weighted images.
weight images. These signal intensity characteristics are indicative of mild T1 shortening due to the proteinaceous serosanguineous serum (40).

When followed sequentially, intratumoral hemorrhage may appear to evolve more slowly than parenchymal hematomas, reflecting the much lower ambient oxygen levels (57). Delayed evolution of hematomas is, therefore, seen both in the setting of low O2 (not enough to oxidize the heme iron from ferrous deoxyhemoglobin to ferric methemoglobin) and high O2 (which keeps the methemoglobin reductase systems powered to drive methemoglobin back to deoxyhemoglobin). The optimal O2 tension for hemoglobin oxidation is approximately 20 mm Hg (58).

When tumors bleed in the brain, macrophages move in to surround the hemorrhage just as in the non-neoplastic situation. Hemosiderin or ferritin rims are seen in the chronic setting. With renewed tumor growth, the hemosiderin rim may become disrupted (47) (Fig 15). While this is a useful sign of neoplastic hemorrhage, it is less than 100% specific because rebleeding from any cause—for example, hypertension—can produce disruption of an earlier hemosiderin rim.

**SUMMARY**

Although CT may be more useful for detecting hyperacute parenchymal hemorrhage or early subarachnoid or intraventricular hemorrhage, MR is certainly more sensitive after 12–24 hours. MR is also more specific than CT in determination of the age of the hemorrhage. Hemorrhage passes through five well-defined and easily identified stages on MR images as it evolves. Knowledge of these stages may be useful to date a single hemorrhagic event or to suggest that multiple hemorrhagic events have occurred at different times. As stressed throughout this review, it is important to acquire both T1- and T2-weighted images to adequately characterize and stage hemorrhage.

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